FUNCTIONAL CONNECTIVITY COMPARISON BETWEEN HEAD-DOWN TILT BED REST AND MICROGRAVITY DURING SPACEFLIGHTS

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INTRODUCTION

In the course of space travel, the central nervous system (CNS) encounters a variety of environmental stress factors [1, 2]. Microgravity is considered the primary factor influencing the brain, acting through various mechanisms such as weightlessness, vestibular deprivation or cephalic fluid shift [1]. On Earth, head-down tilt **bed rest** (HDBR) is a commonly used technique, as it is considered a spaceflight analogue that mimics the effect of microgravity in the cardiovascular system.

We have studied how the brain functional connectivity (FC), calculated from electroencephalography (EEG) recordings, is affected during spaceflights and HDBR experiments. FC quantifies the synchronization between two or more brain areas, and is generally studied in different neural networks such as the default mode network (DMN), or all cortical and subcortical regions mapped by the AAL atlas (here named as whole brain network -WBN), among others [3]. To study these changes, we have compared EEG data recorded before, during and after spaceflight/bed rest (see timeline in *poster ID: 1648549*).

MATERIALS & METHODS NEUROSPAT data 32 channels NEUROSPAT data 55 channels HDBR data 32 channels Source reconstruction using eLORETA method Calculate the PLV (phase locking value) matrix for each subject and condition

Calculate the Strength matrix for each PLV matrix

The main objective of this study was to compare the **NEUROSPAT** experiments [4] with **HDBR** findings [5], to elude possible neurophysiological differences between those two experimental conditions.





Figure 1. Changes in strength (FC-eyes closed) between conditions in the NEUROSPAT experiment (55 electrodes). The bar graph depicts the mean±SEM of the (A) WBN theta band, (B) WBN beta band, (C) DMN alpha band, (D) DMN beta band, FC strength for each condition (*p<0.05).

Figure 3. Changes in strength (FC-eyes closed) between conditions in the NEUROSPAT experiment (32 electrodes). The bar graph depicts the mean±SEM of the (A) WBN theta band, (B) WBN beta band, (C) DMN alpha band, (D) DMN beta band, FC strength for each condition (*p<0.05).

Whole Brain Network – β band (q values)



Figure 2. Brain figures represent the areas with higher statistical differences in the beta band when comparing ROIs. (A) pre-fight vs. in-fight conditions, (B) in-fight vs. post-fight conditions, (C) pre-fight vs. post-fight conditions. The colorbar is displayed as a family-wise corrected significance level of q value > 4, corresponding with a minimum p value of 0.05.



Figure 4. Changes in strength (FC-eyes closed) between conditions in the HDBR experiment (32 electrodes). The bar graph depicts the mean±SEM of the (A) WBN theta band, (B) WBN beta band, (C) DMN alpha band, (D) DMN beta band, FC strength for each condition (*p<0.05).

		CONCLUSIONS		
Inflight: $\uparrow \beta$ FC in the leftInflight: $\uparrow \beta$ angular gyrussuperior fromInvolved in spatial processingInvolved in spatial	al gyrus NEURO	COSPAT data: \neq HDBR data: reduction \neq of θ and β FC \downarrow of α FC	HDBR data θ and β FC: almost no difference between conditions	s When reducing the NEUROSPAT data to 32 channels: no significant results
(i.e. verticality assessment)[6] memory Adaptative response to the microgravity er	I he HDBR	R analogue capture dissimilar EEG dynamic red to microgravity more data needed	A low number of electrodes is not enough to correctly calculate the FC . As described in <i>poster ID: 1648424</i> at least more than 64 electrodes EEG systems are needed to obtained reliable results	

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